

LARYNGOLOGY

Comparison of electroglottographic variability index in euphonic and pathological voice

Confronto dell'indice di variabilità EGG nella voce eufonica e patologica

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SUMMARY

In a recent study we introduced a new approach for analysis of the electroglottographic (EGG) signal. This method is based on the evaluation of variation of the EGG signal and its first derivative, through new software developed by the Pisan phoniatic school. This software is designed to extract quantitative indices related to the contacting and decontacting phases of the vocal folds during phonation. The software allows us to study the combined variability of vibration amplitude and velocity (i.e. the first derivative of the EGG signal). Pathological voices show a much more variable EGG signal compared to normal voices, since cordal vibration is made irregular due to the presence of glottis plane pathologies. With the aim of demonstrating the differences between normal and pathological voices relevant to combined vibration amplitude and velocity variability, we have introduced a new quantitative parameter named "variability index, VI". We studied 95 subjects (35 normal and 60 with pathological voice); among pathological subjects, 15 showed functional dysphonia and 45 showed organic dysphonia. Subjects affected by organic dysphonia presented: 15 bilateral vocal nodules, 15 unilateral polyps and 15 unilateral cysts. All subjects were studied with videolaryngostroboscopy; electro-acoustic parameters of the voice were analysed with the KayPENTAX CSL (Model 4500) system. The EGG signal was recorded using KAY Model 6103 connected to the CSL system. The new software for the analysis of the EGG signal allows us to obtain not only a VI total value relevant to variability during all the recording, but also partial VI values relevant to the different glottis cycle phases. In fact, plotting the amplitude variation and its first derivative on a Lissajous graph, it is possible to divide the whole glottis cycle into four phases (each represented by four quadrants on the graph): the initial vocal folds contacting activity (VI-Q1), the last phase of vocal folds contacting (VI-Q2), the first phase of vocal folds decontacting (VI-Q3) and the last phase, up to the complete decontacting of vocal folds (VI-Q4). For each quadrant, it is also possible to work out the percent variability index. By comparing the variability indices in the normal and pathological groups, we obtained the following results: the total VI was significantly higher in the pathological subjects (0.25 vs 0.18; $p = 0.01$); the absolute value of VI was higher in pathological subjects, although the difference was not significant (VI-Q2, 0.041 vs 0.029; VI-Q3, 0.065 vs 0.058; VI-Q4, 0.054 vs 0.052). The percent variability in the Q2 quadrant (VI-Q2%) was significantly higher in pathological subjects compared to normal subjects (0.22 vs 0.16) ($p = 0.01$). The results of this study confirm that our new software for analysis of EGG signal can distinguish normal voice from pathological voice based on the new quantitative parameter VI. Moreover, this study emphasises that the final contact phase of vocal folds is the most representative of the difference between the normal and pathological voice and shows a wider variability in terms of amplitude and vibration velocity. Further studies on larger groups of subjects will be required to confirm these results and assess differences in the EGG signal among the various vocal fold pathologies.

KEY WORDS: Electroglottography • EGG • Glottal cycle • EGG variability • Vocal fold dynamics • DEGG

RIASSUNTO

In un recente lavoro abbiamo presentato un nuovo approccio allo studio del tracciato elettroglottografico; il metodo di studio si basava sulla valutazione della variazione del segnale EGG e della sua derivata prima, mediante un nuovo software ideato dalla scuola foniatrica pisana. Tale software permette di ottenere indici quantitativi relativi alle fasi di contatto e decontatto delle corde vocali durante la fonazione, mediante lo studio della variabilità combinata dell'ampiezza e della velocità di vibrazione (derivata prima del segnale EGG). La voce patologica presenta un segnale EGG più variabile rispetto alla voce normale: la vibrazione cordale è resa irregolare dalla presenza di

patologia del piano glottico. Al fine di dimostrare differenze tra voce normale e patologica relative alla variabilità combinata tra ampiezza e velocità di vibrazione, abbiamo introdotto un nuovo parametro quantitativo denominato "variability index, VI". Abbiamo studiato 95 soggetti (35 normali e 60 con voce patologica); tra i patologici, 15 mostravano disfonia disfunzionale e 45 disfonia organica. I soggetti affetti da disfonia organica presentavano: 15 noduli vocali bilaterali, 15 polipi unilaterali e 15 cisti unilaterali. Tutti i soggetti venivano studiati con videolaringostroboscopia, i parametri elettroacustici della voce venivano analizzati attraverso il sistema KayPENTAX CSL (Model 4500). L'esame EGG veniva effettuato attraverso il KAY Model 6103 collegato al sistema CSL. Il nuovo software di analisi del segnale EGG permette non solo di ottenere un VI totale (VI-total) relativo alla variabilità durante tutta la registrazione, ma anche VI parziali relativi alle varie fasi del ciclo glottico. Applicando la variazione di ampiezza e della derivata prima su un grafico di Lissajous, è possibile dividere l'intero ciclo glottico in 4 fasi (rappresentate da 4 quadranti nel grafico): la fase iniziale di contatto delle corde vocali (VI-Q1), la fase finale di contatto delle corde vocali (VI-Q2), la fase iniziale di de-contatto delle corde vocali (VI-Q3) e la fase finale, fino al completo de-contatto delle corde vocali (VI-Q4). Per ciascun quadrante, inoltre, è possibile calcolare l'indice di variabilità percentuale. Comparando gli indici di variabilità nei gruppi normali e patologici, abbiamo ottenuto i seguenti risultati: il VI totale era significativamente maggiore nel gruppo di soggetti patologici (0,25 vs 0,18; $p = 0,01$); il valore assoluto di VI in 3 quadranti era maggiore nei patologici anche se non in maniera statisticamente significativa (VI-Q2, 0,041 vs 0,029; VI-Q3, 0,065 vs 0,058; VI-Q4, 0,054 vs 0,052). La variabilità percentuale del quadrante Q2 (VI-Q2%), era significativamente più elevata nei soggetti patologici rispetto ai normali (0,22 vs 0,16) ($p = 0,01$). I risultati di questo studio hanno confermato che il nostro nuovo software di analisi del tracciato EGG permette di distinguere la voce normale da quella patologica sulla base di un nuovo parametro quantitativo, il VI. Lo studio mette in evidenza come la fase che più caratterizza la differenza tra voce normale e patologica è quella relativa alla fase finale di contatto delle corde vocali, che presenta una maggiore variabilità di ampiezza e velocità di vibrazione. Ulteriori studi, con un numero maggiore di soggetti, saranno necessari per confermare questi risultati e per dimostrare eventuali differenze di variabilità del segnale EGG nelle diverse patologie delle corde vocali.

PAROLE CHIAVE: *Elettroglottografia • EGG • Ciclo glottico • Variabilità EGG • Dinamica delle corde vocali • DEGG*

Introduction

Electroglottography (EGG) is an electrical impedance-based technology for inferring vocal folds contact during phonation¹⁻³. This technique is based on the principle that electrical impedance through the neck systematically varies with the degree of contact of vocal folds in the glottic cycle. The complete contact of vocal folds is associated with low impedance values and a high electric current flow through the glottis. As the contact of vocal folds decreases (decontacting phase), the high impedance of air through the glottic plane causes a significant variation of the current flow; as a consequence, the voltage passing through neck tissues reduces. These voltage variations which occur during phonation in the vocal folds' edge contact and detachment phases are at the basis of the EGG signal. Electroglottography is carried out using two electrodes placed on thyroïdal cartilage. Electric current with low voltage and intensity (0.5 V; < 10 mA) and high frequency (0.3-5 MHz) flows through the electrodes, whereas the neck acts as a variable resistor in a constant current circuit⁴.

From a clinical standpoint, the advantages of EGG are as follows: the EGG cycle is repeated at each contact and its frequency is considered the most accurate indicator of the voice fundamental frequency (F0)⁵⁻⁷; the EGG plot demonstrates the best indirect representation of the vocal fold vibration as a whole and particularly during its closing phase^{5,7,8}; when used with high-speed imaging and acoustic analysis, EGG is able to highlight irregular vibratory patterns⁹. In the early 1990s, Ursino and colleagues correlated

EGG findings with subglottic pressure variations measured in vivo, obtaining important information on cordal vibration physiology^{10,11}. Hosokawa et al. have recently shown how EGG parameters related to the regularity of vocal fold vibration may be useful for diagnosis of dysphonia and assessment of the efficacy of voice therapy¹². Somanath and Mau confirmed that EGG parameters may serve as a marker for treatment response and found that they may provide a within-subject measure of vocal strain; adding EGG to multidimensional assessment may improve characterisation of voice disturbance¹³. Moreover, EGG is useful for the voices of singers in the study of diplophonia and vibrato (in conjunction with spectrography) and for the training of singers (displaying the contact quotient associated with the trend of F0 in real-time). Finally, EGG examination is simple, inexpensive and non-invasive^{6,14-16}.

It should be stressed that the EGG signal is influenced by many factors that alter the electric impedance through the neck, such as larynx extrinsic muscle contraction, variations of larynx position during phonation and degree of dilatation of large neck vessels. These variables can, however, be removed by high-pass filtering of the raw EGG signal. Other potential factors for impedance variation include: excess adipose tissue in the neck that may obstruct the recording of the EGG signal, or the presence of mucus strands which may act as a direct path for current flow through the open glottis, thus simulating vocal fold contact. Besides these limits, EGG shows other disadvantages: large variability among individuals prevents the definition of pathological and normal voice and the definition

of the type of pathology; the EGG signal does not contain information either about the glottal area during opening or the air flow that passes through or the side which is possibly affected by pathologies (left or right). Moreover, the EGG cannot measure the amplitude of the mucosal wave or the anterior-posterior asymmetry, because it is a cumulative measurement of the vocal fold contact for all points that pass through the glottis^{4,5,17}.

The EGG signal as it is still currently analysed is significant only when vocal folds have a certain degree of contact and does not specify the point where the contact itself is taking place. Moreover, the simple EGG signal does not provide any information to allow precise determination of the moment at which the vocal folds contact starts as well as the moment in which their separation starts^{4,18}. For this reason, the EGG signal has been generally subdivided into a “contact phase” (which includes both phases of increase and reduction of the vocal fold contact) and a “minimal contact phase” (which includes all the phases of apparent missing contact of the vocal folds)⁴. Based on these limits, several quantitative parameters related to the closure phase have been developed to describe the EGG signal. Among these, “contact quotient” (CQEGG) (ratio of contact phase duration to the fundamental period) is worth mentioning^{19,20} and the “contact index” (difference between increasing and decreasing vocal fold contact durations, divided by total contact phase duration)²⁰.

In fact, the EGG is a one-dimensional signal obtained from the complex three-dimensional motion of the vocal folds. The speed of such motion is strictly related to the contacting and decontacting phases of the vocal folds activity. The first mathematical derivative of the EGG waveform (DEGG) represents the speed of change of the EGG with time⁵. It is a common assumption that the maxima found in the DEGG signal always coincide with the moments of glottal closure and opening; thus, the exact timing of glottal closure can be easily obtained from a single maximum in the DEGG signal^{21,22}. Some recent findings suggest that DEGG peaks do not always coincide with the events of glottal closure and initial opening. Vocal fold contacting and decontacting do not occur at infinitesimally small instants of time, but extend over a certain interval (0.24-10.88%), particularly under the influence of anterior-posterior phase differences²². Nevertheless, the EGG and its first derivative are rich in useful information about the vocal folds activity, which is the result of the complex process of phonation at larynx level. Already in the early 1990s, Ursino and colleagues studied the correlation between the EGG signal and its first derivative using the Lissajous curve²³. The wider dispersion in the graphs obtained using the Lissajous curve, typical of a wider variability of the EGG and its prime derivative (and

thus wider variation in the velocity of vibration), proved to be typical of pathological voices. Ursino's work takes credit for stressing the importance of studying the correlation between EGG and DEGG in the investigation of normal and pathological voices, even though the limits set by that signal processing approach did not allow to determine the dispersion and, consequently, to discriminate euphonic voice from dysphonic voice²³.

Dysphonia caused by vocal fold lesions, paralyses and other pathological conditions are generally associated with a greater irregularity of the EGG signal. Many of these instabilities in the signal are related to the intrinsic non-linearity in the vibration of the vocal folds. These irregularities are thought to arise from the intrinsic nonlinearity of the vocal system and have been extensively examined by the theories of non-linear dynamics²⁴. Using the non-linear dynamic methods, it was possible to quantitatively describe the regular and irregular dynamics of the vocal folds, such as in asymmetric vocal folds and polyps^{25,26}. Moreover, this approach was successfully employed to characterise different “vibratory states” of the vocal folds occurring during the transition between modal and falsetto voice²⁷.

In a recent work, we presented a new approach for the analysis of the electroglottographic signal; the method of this study is based on the EGG signal and its first derivative; which allows the extraction of quantitative indices about the EGG activity during the contacting-decontacting phases of the vocal folds process during steady-state vocal tests²⁸. We carried out EGG analysis of 21 normal and 21 pathological voices, considering the variability based on the combined amplitude-velocity analysis, in order to demonstrate any quantitative differences between pathological and normal subjects. In normal subjects, the global variability index (VI) (expression of Amplitude and Velocity variation) was definitely lower than in pathological subjects. Despite the small sample, the above method for analysing the EGG signal proved to be efficient in discriminating normal subjects from pathological ones²⁸. The aim of this work is to confirm from a clinical point of view the data from our previous study using a larger study group, and to assess and evaluate possible differences between the various pathologies.

Materials and methods

A total of 95 subjects were enrolled and divided into two groups (35 normal subjects and 60 pathological subjects); among pathological subjects, 15 showed functional dysphonia, 45 showed organic dysphonia. Subjects affected by organic dysphonia presented: 15 bilateral vocal nodules, 15 unilateral polyps and 15 unilateral cysts.

All subjects were studied with videolaryngostroboscopy (KayPENTAX RLS 9100 Digital Strobo). Parametric analysis of voice quality during phonation of the “a” vowel was performed using Multidimensional Voice Program (MDVP) (KayPENTAX CSL Model 4500). Spectrographic analysis was carried out during prolonged phonation of the vowel “a” with the CSL Main Program (KayPENTAX CSL Model 4500). Laryngeal electroglottography (KAY Model 6103) was performed on all subjects while phonating the “a” vowel at a comfortable pitch and loudness.

EKG and amplitude-speed combined analysis of electroglottographic signal variability

In clinical audiological lab, the electroglottographic signal is commonly recorded using commercial instrumentation (in our case KAY Model 6103) through two metallic electrodes positioned at the left and right side of the throat at the level of the vocal folds.

Variations in the position of the electrodes, muscular activity and movement of the other neck tissues may cause “noise” in the EGG signal which appears as low frequency baseline drift, high frequency noise and artefacts. To limit this “noise”, an accurate protocol for signal acquisition needs to be adopted in the laboratory: accurate position of electrodes, fixed and relaxed position of the subject, choice of simple vocal test and with short duration, subject awareness regarding the test to be performed and the actions to be avoided. Despite these precautions, some noise could still be present in the signal; signal pre-processing has to be carried out to reduce residual artefacts and enhance the real EGG component.

The EGG signal was obtained from commercial instrumentation in the form of a standard WAV file with a sampling rate of 44 kHz. In each recording, a sub-interval of 7 seconds was selected by visual inspection of the EGG signal according to the presence of noise/artefacts and amplitude stability.

All signal processing was done using the software package MatLab Vers. R2012a-Win64 (Mathworks Inc.). The EGG signal recorded during a continuous vocal phonation was processed in order to obtain the first derivative, which is related to the velocity of the contacting change of the vocal folds. The average fundamental frequency was computed and its corresponding period was taken as the typical duration of the EGG cycle. After each glottal cycle was identified, the EGG signal and its derivative are locally normalised in time²⁸. It is therefore possible to obtain a graphic representation of both the EGG filtered signal (red line) and its first derivative (speed of change of the EGG with time) (blue

line). The lighter red and blue areas around the main lines represent the variability of the EGG signal and its first derivative (Fig. 1).

Besides the above-mentioned graph, for each glottal cycle the amplitude and related velocity signals can be plotted on an X-Y axis, thus forming a multi-layer display where each EGG cycle appears as a circular trace. This X-Y representation can be viewed as a polar graph: by increasing the angle from 0 to 360° with incremental steps corresponding to the time normalisation re-sampling of the EGG cycle, mean value and standard deviation (SD) are computed. The results are the amplitude-velocity mean cycle curve and the related SD curve. The shape of the mean loop is strictly associated with the relationships between amplitude-velocity changes and phonation phases. The surrounding area represents the variability of local vocal phenomena around the above mean curve. Besides the bi-dimensional representation just described, the signal can be plotted on an X-Y-Z graph (3D representation): the traces are formed by points where the X coordinate corresponds to the EGG samples, Z coordinate is the corresponding first-derivatives and Y is time. The different colours of the traces (from dark blue to red) show the time flow (Figs. 2, 3).

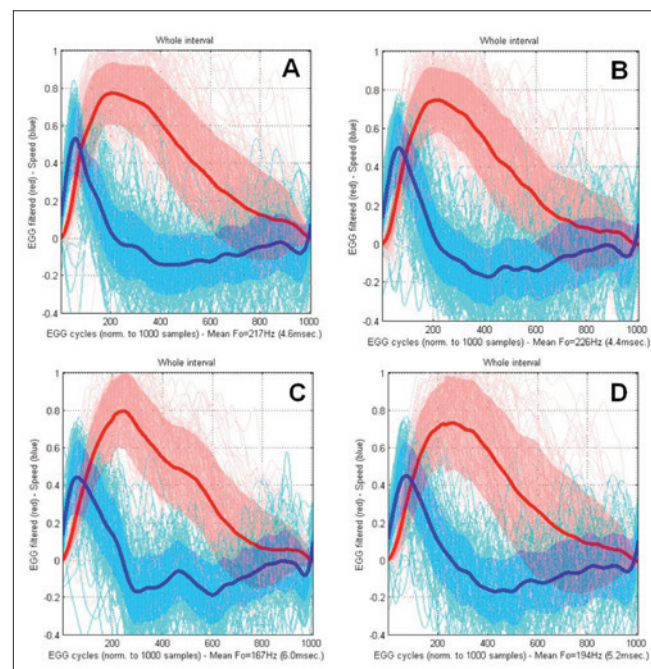


Fig. 1. Graphic representation of both EGG filtered signal (red) and its first derivative (speed of change of the EGG with time) (blue) in patients of study group (A: Functional; B: Bilateral nodules; C: Polyp; D: Cyst). The lighter red and blue areas around the main lines compared to main lines (representation of the variability of the EGG signal and its first derivative) are more evident than in the normal control.

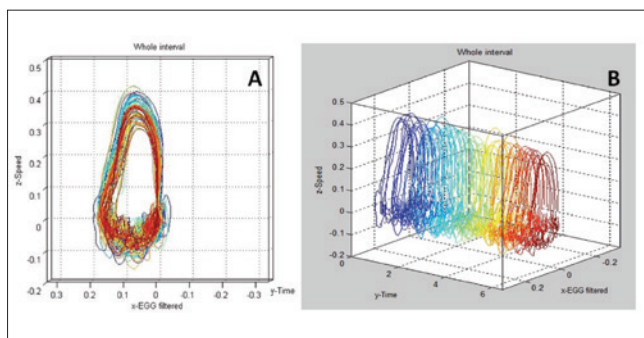


Fig. 2. X-Y plot of synchronised EGG cycles in 2D (A) and in 3D (B) version in a normal subject; the traces are formed by points where the X coordinates are the EGG samples, Z are the corresponding first-derivatives and Y are the time. The different colour (from dark blue to red) of the traces shows the time flow.

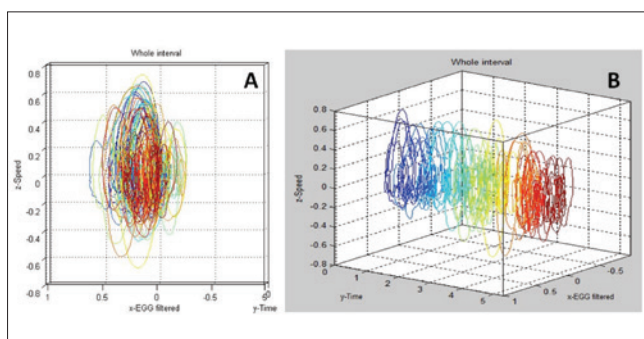


Fig. 3. The same representation as Fig. 2, in a patient with pathological voice (Cyst).

The phonation process can be characterised in more detail by computing couples of indices (mean and standard deviation) as obtained by dividing the polar graph in 4 quadrants, approximately associated with the different phases of the glottal cycle (Fig. 4)²⁸. Since each quadrant is associated with a specific behaviour of the vocal folds, four variability indices VI were extracted, one for each quadrant. The quadrants are numbered clockwise starting from the top-left position. These indices offer a compact view of the variability of the glottal waves in significant physiological phases. Variability in each quadrant can be calculated as both absolute value and a percentage of the total value. The parameters are therefore represented by the following:

- VI-Q1 and VI-Q1%: during the initial vocal folds contacting activity;
- VI-Q2 and VI-Q2%: during the last phase of vocal folds contacting;
- VI-Q3 and VI-Q3%: during the first phase of vocal folds decontacting;

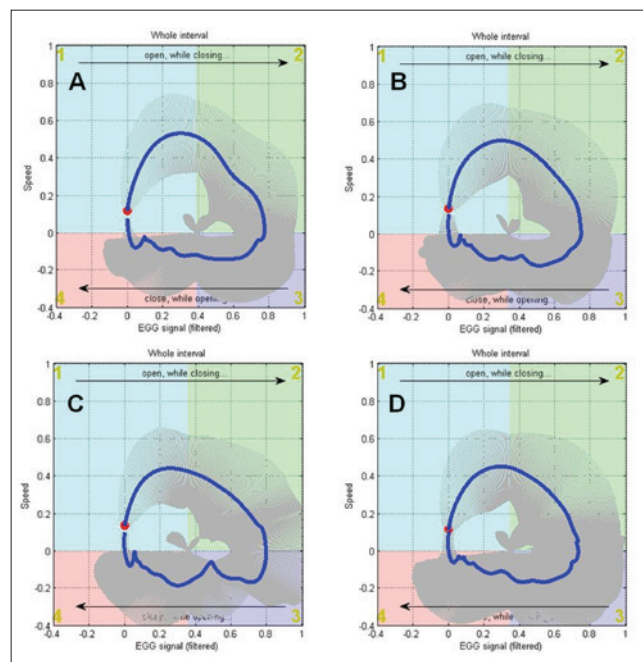


Fig. 4. EGG representation of the phonation process at vocal folds level in pathological voice (A: Functional; B: Bilateral nodules; C: Polyp; D: Cyst). The figure is divided in 4 quadrants corresponding to different phases of the glottal cycle. The blue trace represents the mean EGG cycle, starting from the red circle. The grey segments crossing the blue line are the SD of normalised cycles, which is the variability of the EGG process.

- VI-Q4 and VI-Q4%: during the last phase, up to the complete decontacting of vocal folds.
- Finally, a total variability index VI-tot is computed²⁸.

Statistical analysis

The data were analysed using SPSS v.21.0 (IBM Corp., Armonk, NY, USA) and the results were considered significant for p values < 0.05.

Categorical variables were expressed as percentages, whereas continuous variables were expressed as interquartile range (Median; IQR; Min and Max). In the first step, the Kolmogorov-Smirnov test was performed²⁹ to verify the normality and the homoscedasticity of quantitative variables (VI-tot, VI-Q1, VI-Q1%, VI-Q2, VI-Q2%, VI-Q3, VI-Q3%, VI-Q4, VI-Q4%). The VI-tot, VI-Q1%, VI-Q3, VI-Q4 and VI-Q4% variables resulted in a normal distribution, opposite to, the VI-Q1, VI-Q2, VI-Q2% and VI-Q3% parameters. For this reason, we employed median values and non-parametric tests in the comparison between normal vs. pathological subjects. Mann-Whitney U statistic (non-parametric for two independent comparison) was performed to compare the median of different variables (VI-tot, VI-Q1, VI-Q1%, VI-Q2, VI-Q2%, VI-Q3, VI-Q3%, VI-Q4, VI-Q4%) between normal and pathological groups.

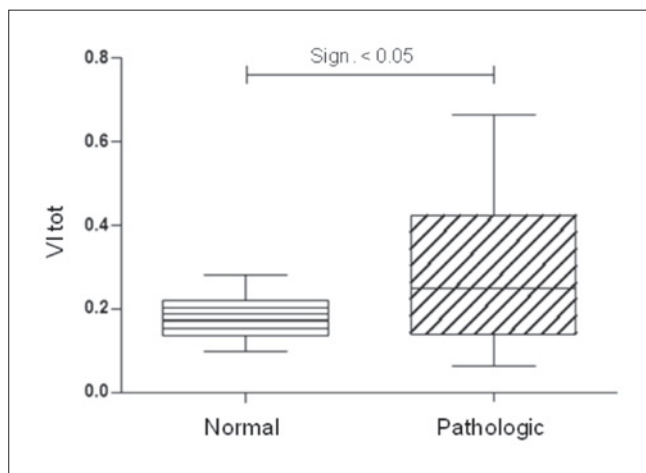


Fig. 5. VI-tot values sorted by normal and pathologic population. The box plot diagram shows the distribution of median, interquartile range, minimum and maximum, and outlier observed values.

Results

Normal vs Pathological

Comparing the variability indices in the normal and pathological groups, we obtained the following results: the total VI showed significantly higher values in the pathological group ($p = 0.01$) (Fig. 5). As far as the absolute values are concerned (VI-Q1, VI-Q2, VI-Q3, VI-Q4), a significant difference was not observed, even though the absolute VI-Q2, VI-Q3 and VI-Q4 values were higher in the pathological group compared to the normal group (VI-Q2, 0.041 vs 0.029; VI-Q3, 0.065 vs 0.058; VI-Q4, 0.054 vs 0.052). It should be emphasised that the difference VI-Q2 was at the boundaries of significance.

The percent variability in each quadrant VI-Q2% was significantly higher in the pathological group ($p = 0.01$); VI-Q1% and VI-Q4% were higher in the normal group ($p = 0.01$ and $p = 0.02$ respectively). The VI-Q3% value difference was not statistically significant.

Data relevant to the difference in the variability indices are summarised in Table I.

Discussion and conclusions

EKG is a non-invasive method that indirectly monitors vocal folds vibration by measuring the electrical impedance in the electrodes placed on the dermis above the thyroïdal cartilage. In this way, EKG indirectly measures contact extension between the two vocal folds^{1,2}. To date EKG stands out as the most representative, although indirect, investigation of vibration of the vocal folds, particularly as far as the closure phase is concerned^{7,8}. Notwithstand-

ing its advantages, EKG suffers from some limitations. In particular, variability of the EKG signal makes the distinction between pathological and normal voices difficult, as well as impossible to distinguish the various types of pathologies of the glottic plane. In fact, the EKG wave is easily influenced by both the normal variations of the cordal vibration and by mucus strands across the glottis^{5,17}. The EKG signal, as it is currently analysed, is significant only when vocal folds have a certain degree of contact; however, it does not specify the point where contact occurs. Moreover, the simple EKG signal does not provide any information to precisely determine the moment at which the vocal fold contact begins or the moment at which the vocal folds start to separate^{4,18}.

Several physical and mathematical models have been employed to identify EKG signal landmarks, which should represent physiological and morphological aspects of cordal vibration. Many of those techniques offer a detailed vision of the cordal vibration process, yet the operator is required to carry out morphological analysis and visual inspection of the curves obtained³⁰.

In fact, the EKG is a one-dimensional signal obtained from the complex three-dimensional motion of the vocal folds. The speed of such motion is strictly related to the contacting and decontacting phases of the vocal folds activity. The first mathematical derivative of the EKG waveform (DEKG) represents the speed of change of the EKG with time⁵.

The EKG wave and the behaviour of its prime derivative are rich in information about vocal folds activity. In particular, quantitative analysis of the combined variability of amplitude and velocity in the EKG graph may offer a precious tool to evaluate the actual behaviour of the vocal folds in normal and pathological voices²⁸. In one of our previous studies, we illustrated a new approach to elaborate data obtained from the electroglottographic signal. This method is based on the combined analysis of the EKG signal and its prime derivative; this allows calculation of quantitative indices related to electroglottographic activity during the contacting-decontacting phases of the vocal folds process in steady-state vocal tests. In particular, we have worked out the variability index (VI), which represents the combined variation in amplitude and velocity of the EKG signal²⁸.

The results of this preliminary study on 21 euphonic subjects and 21 dysphonic subjects showed that VI could distinguish normal voice from pathological voice.

In the present study, we have broadened the sample of both normal and pathological subjects, with the aim of confirming from a clinical standpoint the results obtained from our previous work, as well as identifying and evaluating eventual differences among the various pathologies. The results herein, carried out on 95 subjects (35 euphonic

Table I. Differences in variability indices between normal and pathological subjects.

		N	Median	IQR	Min	Max	Mann-Whitney U test	
VI-tot	Normal	35	0.18	0.14	0.22	0.10	0.28	0.01
	Pathologic	60	0.25	0.14	0.42	0.07	0.67	
VI-Q1	Normal	35	0.03	0.02	0.04	0.01	0.05	0.77
	Pathologic	60	0.03	0.02	0.05	0.00	0.08	
VI-Q1%	Normal	35	0.15	0.13	0.19	0.04	0.27	0.01
	Pathologic	60	0.12	0.08	0.15	0.00	0.42	
VI-Q2	Normal	35	0.03	0.02	0.04	0.01	0.10	0.07
	Pathologic	60	0.04	0.02	0.17	0.01	0.66	
VI-Q2%	Normal	35	0.16	0.13	0.20	0.11	0.39	0.01
	Pathologic	60	0.22	0.15	0.41	0.07	0.99	
VI-Q3	Normal	35	0.06	0.05	0.08	0.02	0.12	0.34
	Pathologic	60	0.07	0.05	0.10	0.00	0.20	
VI-Q3%	Normal	35	0.34	0.32	0.38	0.13	0.46	0.09
	Pathologic	60	0.33	0.26	0.36	0.00	0.48	
VI-Q4	Normal	35	0.05	0.05	0.07	0.04	0.13	0.73
	Pathologic	60	0.05	0.04	0.08	0.00	0.17	
VI-Q4%	Normal	35	0.30	0.29	0.36	0.21	0.46	0.02
	Pathologic	60	0.29	0.19	0.34	0.00	0.48	

and 60 pathological), confirm that the total variability index (VI-tot), which represents the global variability of the recorded signal, turns out to be a higher index in dysphonic subjects than in the control group ($p = 0.01$). The study of the variability indices in each quadrant, representing the different phases of the glottic cycle (initial vocal folds contacting activity; last phase of vocal folds contacting; first phase of vocal folds decontacting; last phase up to the complete decontacting of vocal folds), showed a significant difference for VI-Q2% ($p = 0.01$), and at the boundaries of significance for VI-Q2, evidence of a higher signal disturbance during the last phase of vocal folds contacting in a pathological subject. In fact, the study group included 45/60 organic dysphonias (bilateral nodules, unilateral polyps and unilateral cysts), for which it is conceivable that the last phase of vocal folds contacting was the most disturbed one. The absolute values in the other quadrants (VI-Q1, VI-Q3, VI-Q4) were not significantly different way between normal and pathological subjects. This result confirms the above assumptions, i.e. that combined variability of amplitude and velocity of the EGG is higher only during the last phase of vocal folds contacting. The percent variability index in the single quadrants reflects the percentage index of variability in each phase of the glottis cycle in relation to the total variability. In our study, the VI-Q2% was clearly higher in pathological subjects than in normal subjects; on the other hand, the remaining percentage indices (VI-Q1%, VI-Q3%, VI-Q4%) were clearly higher in normal subjects than in pathological subjects. For

this reason, being VI-tot higher in pathological subjects, the percentage value to be considered as significant is VI-Q2%. Due to the limited size of the samples of each pathological subgroup, it was not possible to perform a statistical evaluation aimed at pointing out potential differences between organic or functional dysphonia and various patterns of the EGG signal among the several organic pathologies. Further studies on larger groups of subjects will be required to confirm these results, assess any quantitative difference in the various phases of the glottal cycle and to highlight any difference in EGG signal among the various vocal fold pathologies.

Conflict of interest statement

None declared.

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